

# Blood compatibility improvement of titanium oxide film modified by doping La<sub>2</sub>O<sub>3</sub>

Lin Zhang · Dihu Chen · Keqiang Wang ·  
Fengmei Yu · Zhanyun Huang · Shirong Pan

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**Abstract** La<sub>2</sub>O<sub>3</sub> doped titanium oxide (TiO<sub>2</sub>) films with different concentration were deposited by means of the Radio-Frequency magnetron sputtering technique. The microstructure and surface properties of TiO<sub>2</sub> films were characterized by X-ray diffraction (XRD), X-ray photoelectron spectroscopy (XPS) and contact angle test. The blood compatibility of the specimens was evaluated by tests of platelet adhesion. Results show that pure rutile phase is formed in doped samples and La<sub>2</sub>O<sub>3</sub> incorporation significantly improves the wettability and hemocompatibility of TiO<sub>2</sub> films. Our studies demonstrate that La<sub>2</sub>O<sub>3</sub> doped TiO<sub>2</sub> films are potentially useful biomaterials with good blood compatibility.

## 1 Introduction

TiO<sub>2</sub> thin films have been widely investigated in photocatalysis application fields such as hydrophilicity, self-cleaning and purification of air and toxic gases, etc. Recent

studies have shown that TiO<sub>2</sub> films are suitable as surface coatings on biomedical applications due to its good hemocompatibility [1, 2] and researches concerning biomedical aspects are widely increasing [3–5]. Besides the pure TiO<sub>2</sub>, doping TiO<sub>2</sub> films with selective elements is an attractive method to enhance the biological properties of TiO<sub>2</sub> [6, 7]. Rare earth elements exhibit relatively low toxicity, anticoagulant, antiemetic, antiseptic, immunomodulatory and antineoplastic properties, which have aroused considerable interest in medicine application due to these and other pharmacological effects [8]. However, there have rarely been reported on the haemocompatibility of rare earth oxide or/and materials doped with rare-earth elements [9, 10]. In this work, TiO<sub>2</sub> films doped with La<sub>2</sub>O<sub>3</sub> were prepared using RF-magnetron sputtering. The effects of La<sub>2</sub>O<sub>3</sub> incorporation on the structural properties and the hemocompatibility of TiO<sub>2</sub> films were studied. The unique hemocompatibility properties of La<sub>2</sub>O<sub>3</sub> doped TiO<sub>2</sub> films reveal the potential applications in blood-contacting biomedical materials.

## 2 Experiment

The La<sub>2</sub>O<sub>3</sub> doped TiO<sub>2</sub> films were deposited on silicon substrates using RF-magnetron sputtering. The targets were mechanically composted by using TiO<sub>2</sub> powder (in purity 99.9%) and La<sub>2</sub>O<sub>3</sub> powder (in purity 99.5%) with the La<sub>2</sub>O<sub>3</sub> molar concentration of 0%, 1%, 2% and 3%, respectively. Using argon (99.99%) as a sputtering gas, the work pressure was set at 4 Pa. The samples were prepared in room temperature and the RF power of 200 W was applied in the sputtering process. The sample 1, 2, 3 and 4 are prepared using the targets with a doped La<sub>2</sub>O<sub>3</sub> molar content of 0%, 1%, 2% and 3%, respectively.

L. Zhang (✉) · K. Wang · F. Yu  
Information College, ZhongKai University of Agriculture  
and Engineering, Guangzhou 510225,  
People's Republic of China  
e-mail: lin\_phy@163.com

D. Chen · Z. Huang  
State Key Laboratory of Optoelectronic Materials and  
Technologies, and School of Physics & Engineering,  
Sun Yat-Sen University, Guangzhou 510275,  
People's Republic of China

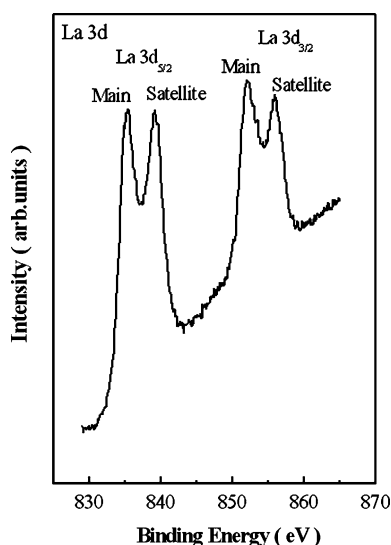
S. Pan  
Artificial Heart Laboratory, The 1st Affiliate Hospital  
of Sun Yat-Sen University, Guangzhou 510080,  
People's Republic of China

The microstructures were evaluated by X-ray diffraction (XRD) with a Cu- $K_{\alpha}$  source under an applied voltage of 40 KV and a current of 40 mA. The compositions were analyzed by X-ray photoelectron spectroscopy (XPS). The contact angle measurement was conducted in atmospheric conditions at room temperature using an OCA20 Optima device. Distilled water and glycol were used in our tests to determine the surface energy and interfacial tension of the samples. Each sample was measured five times on different locations to obtain statistical averages. The experiment of the platelet adhesion was performed to identify the blood compatibility of all the specimens. The reference samples are Chrono flex used in clinical application and glass with good and bad haemocompatibility, respectively [11]. In this experiment, fresh blood of rabbit was centrifugal at 3000 rpm for about 20 min to prepare platelet-rich plasma, and then 0.2 ml of platelet-rich plasma was dropped onto the surface of the samples and incubated at 37°C for 1 h. After incubation, the samples were fixed for 3 hours in glutaraldehyde, critical-point dried with CO<sub>2</sub> and gold coated for examination in a scanning electron microscope. Ten different regions were randomly chosen for each sample to obtain good statistical results.

### 3 Results and discussion

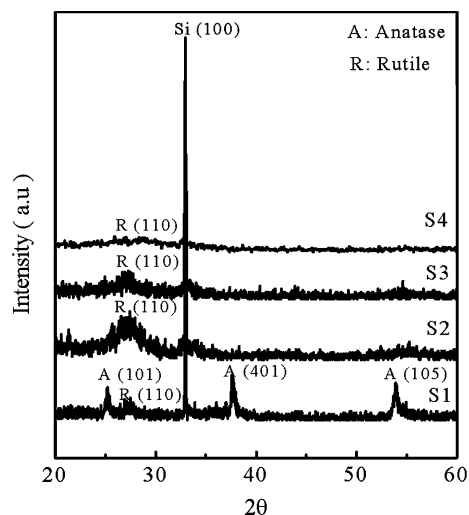
#### 3.1 XPS characterization

The chemical states of La<sub>2</sub>O<sub>3</sub> doped TiO<sub>2</sub> films were investigated by XPS. All the doped samples display the similar results and typical XPS spectrum was shown in Fig. 1. Results indicate that the La 3d spectrum possesses

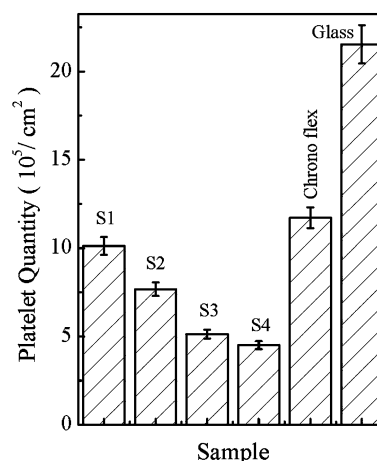


**Fig. 1** Typical La 3d high-resolution XPS spectrum of La<sub>2</sub>O<sub>3</sub> doped TiO<sub>2</sub> films with a content of 2.31 at.%

two doublets and the peaks appearing on the high energy side of the 3d<sub>5/2</sub> and 3d<sub>3/2</sub> peaks are satellite peaks. The most intense peak of La 3d<sub>5/2</sub> is at approximately 835.3 eV, the energy difference between the La 3d<sub>3/2</sub> and 3d<sub>5/2</sub> states is approximately 17 eV, which is agree well with the character values La<sub>2</sub>O<sub>3</sub> [12]. The main peak at 530.5 eV in the O1s spectrum corresponds to O<sup>2-</sup> of the metal oxide. Hence, the XPS results show that La is La<sup>3+</sup> oxidation state, which means that the La exists as La<sub>2</sub>O<sub>3</sub> in TiO<sub>2</sub> films. The La<sub>2</sub>O<sub>3</sub> content calculated from XPS spectra for the La<sub>2</sub>O<sub>3</sub>-doped sample 2, 3 and 4 are approximately 1.56%, 2.31%, and 3.64%, respectively, which are much higher than the content in their corresponding target. The reasons maybe is caused by the difference of sputtering rate between the TiO<sub>2</sub> and La<sub>2</sub>O<sub>3</sub> during deposition.

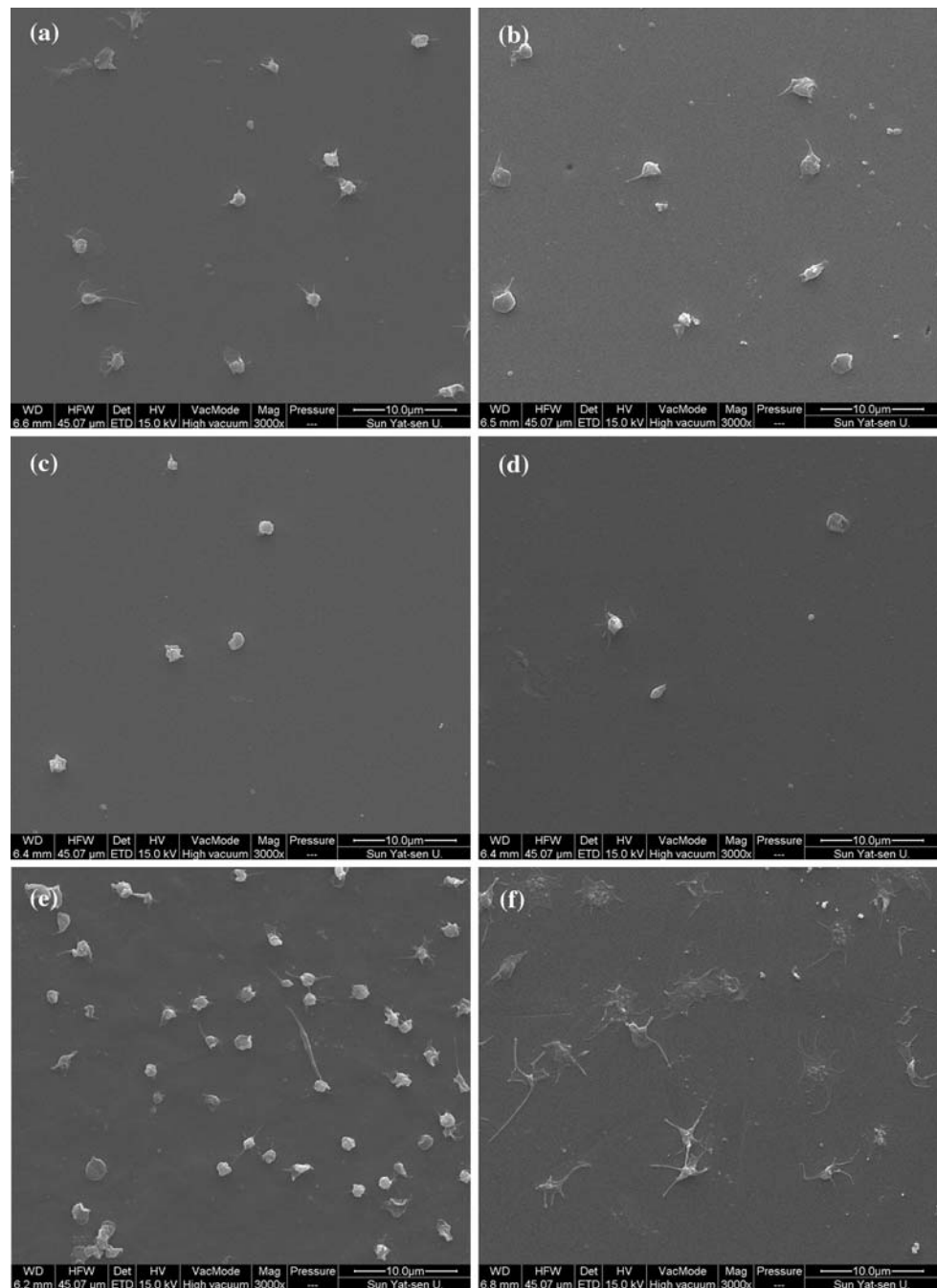


**Fig. 2** XRD pattern of titanium oxide films doped La<sub>2</sub>O<sub>3</sub> with different concentration



**Fig. 3** Number of platelet adhered on the surface of the undoped and La<sub>2</sub>O<sub>3</sub>-doped TiO<sub>2</sub> films with different content

**Fig. 4** Typical SEM images of platelets adhering on the surface of **a** Sample 1; **b** Sample 2; **c** Sample 3; **d** Sample 4 and reference samples of **e** Chrono flex; **f** Glass



### 3.2 XRD analysis

The X-ray diffraction patterns acquired from samples on Si substrate are displayed in Fig. 2. The film on S1 is composed of primarily anatase  $\text{TiO}_2$  (101), (401) and (105), however, pure rutile  $\text{TiO}_2$  (110) can be detected in  $\text{La}_2\text{O}_3$ -doped samples except the Si peak and the width of rutile phase peak becomes much broader with increasing  $\text{La}_2\text{O}_3$  content, indicating that La dopant not only greatly promotes the phase transfer from anatase to rutile and enhances the crystal phase of  $\text{TiO}_2$  with preferential growth

in the direction of (110), but also can refine grain size of  $\text{TiO}_2$ .

### 3.3 Platelet adhesion

The experiments of platelet adhesion have been performed to observe the number and shape of platelet adhered on the surface of the samples. Generally, the sample with less platelet adhered on its surface has better haemocompatibility. The number of platelet adhered on the surface of samples was counted and the statistical results were shown

in Fig. 3. The S1, S2, S3 and S4 are the TiO<sub>2</sub> films with a doped La<sub>2</sub>O<sub>3</sub> molar content of 0%, 1.56%, 2.31% and 3.64%, respectively. Results indicate that there is less platelet adhered on the doped TiO<sub>2</sub> films, exhibiting the excellent haemocompatibility. Typical SEM images of the samples with the adhesion of platelets were shown in Fig. 4. Compared to the undoped TiO<sub>2</sub> film and the Chrono flex, the La<sub>2</sub>O<sub>3</sub> doped samples exhibit fewer platelets aggregation and pseudopod, suggesting that La<sub>2</sub>O<sub>3</sub> doped TiO<sub>2</sub> films are potential in application of blood-contacting biomedical materials.

#### 3.4 Surface energy and interfacial energy results

The first step after blood contacting with the biomaterial is adsorption of plasma protein, which will determines the anticoagulation property of the biomaterial [13]. Adsorption of human fibrinogen (HFG) and human serum albumin (HSA) are two primary factors related to haemocoagulation. It has been proven that adsorption of HFG will promote the adhesion of platelets and activate the platelets, whereas adsorption of HSA does the opposite thing [14]. Therefore, it is important to investigate the interaction between the material surface and plasma proteins. The interfacial tension ( $\Gamma_{HSA}$ ,  $\Gamma_{HFG}$ ) between different proteins (HSA, HFG) and different surfaces were calculated referring to the method in our previous work [11]. In addition,  $\gamma_{sp}^p$  and  $\gamma_{sp}^d$  represent the polar component and dispersive component of the interfacial tension, respectively. The ratio of  $\gamma_{sp}^p/\gamma_{sp}^d$ , which represents the contribution of the polar and dispersive components to the interfacial tension, was evaluated. The calculated results are listed in Table 1.

As shown in Table 1, the contact angles of water decrease with increasing La<sub>2</sub>O<sub>3</sub> concentration, indicating that the doped samples become more hydrophilic with increasing La<sub>2</sub>O<sub>3</sub> content. In addition, the ratio of  $\gamma_{sp}^p/\gamma_{sp}^d$  is from 235.1 to 296.8 in adsorption process of HFG and samples, indicating that polar component ( $\gamma_{sp}^p$ ) is dominant in the interfacial tension compared to dispersive component. Whereas the ratio of  $\gamma_{sp}^p/\gamma_{sp}^d$  is from 1.6 to

12.53 in adsorption process of HSA and samples, suggesting that polar component ( $\gamma_{sp}^p$ ) and dispersive component ( $\gamma_{sp}^d$ ) have almost the same contribution to the interfacial tension. According to the study of C.P. Sharma [15], when the polar and dispersive components have the same contribution to the interfacial tension, the adsorption between protein and biomaterial surface is strong. However, one of the polar and dispersive components is leading in the interfacial tension, the adsorption between protein and biomaterial surface is weak. Therefore, albumin preferentially adsorbs on the doped samples. The result agrees with that of platelet adhesion.

#### 4 Conclusions

La<sub>2</sub>O<sub>3</sub> doped TiO<sub>2</sub> films were deposited using RF-magnetron sputtering. In undoped TiO<sub>2</sub> film, a mixed phase comprising of anatase and rutile was formed. However, in doped TiO<sub>2</sub> films, pure rutile phase was formed. All doped specimens exhibit more hydrophilic surfaces than undoped sample. The better blood compatibility was observed on the La<sub>2</sub>O<sub>3</sub> doped TiO<sub>2</sub> films in comparison with undoped TiO<sub>2</sub>. This may attribute to different contribution of the polar and dispersive components to interfacial tension between materials and proteins. However, more basic studies are needed.

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**Table 1** Contact angle, surface energy components and interfacial tension towards plasma proteins

Samples	Contact angle (degrees)	Interfacial tension(dyn/cm)			
		$\Gamma_{HSA}$	$\gamma_{sp}^p/\gamma_{sp}^d$	$\Gamma_{HFG}$	$\gamma_{sp}^p/\gamma_{sp}^d$
Sample 1	83.1	9.97	12.53	11.85	235.1
Sample 2	81.6	9.46	1.6	11.69	259.9
Sample 3	78.3	7.82	17.7	9.49	279.4
Sample 4	76.5	7.96	10.8	10.8	296.8

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